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Creators	Alexander, Jill, Selfe, James, Greenhalgh, Olivia and Rhodes, David

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Exploratory evaluation of muscle strength and skin surface temperature responses to contemporary cryotherapy modalities in sport

Jill Alexander^{a,*}, James Selfe^b, Olivia Greenhalgh^{a,b} and David Rhodes^c

^aSport, Nutrition and Clinical Sciences, School of Sport and Health Sciences, University of Central Lancashire, Preston, UK

^bHealth, Psychology and Communities, Manchester Metropolitan University, Manchester, UK ^cInstitute for Coaching and Performance (ICaP), School of Sport and Health Sciences, University of Central Lancashire, Preston, UK

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Abstract.

BACKGROUND: The effects of contemporary cryo-compression devices on function are limited compared to traditional applications of cooling. Development of cooling protocols are warranted.

OBJECTIVE: To investigate the effects of three different cryo-compressive modalities applied at the knee on the isokinetic strength of the quadriceps over a re-warming period.

METHODS: Eleven healthy male participants took part (23 ± 14 years; 78.3 ± 14.5 Kg; 180 ± 9.5 cm) randomly assigned to receive all modalities (Game Ready[®] (GR), Swellaway[®] (SA), Wetted Ice (WI)) applied for 15-min, separated by 1-week. Skin surface temperature (T_{sk}) via thermography and the concentric peak moment (PM) of the quadriceps at 60 and 180° /s were collected pre-, immediately-post and at 20-min post-intervention.

RESULTS: Significant reductions occurred in T_{sk} across all timepoints for all modalities ($p \equiv \leq 0.05$). Significant reductions in PM for WI were noted across all timepoints and PM for GR and SA immediately-post ($p \equiv \leq 0.05$) only.

CONCLUSION: Precaution for immediately returning to sport following cryotherapy is required and influenced by type of cooling on muscle strength responses. Alternate targeted treatment modalities to minimise deferred deleterious effects on muscle strength may be considered. Research into length of application, periodisation and location is warranted for the development of such contemporary cryo-compressive modalities in applied practice.

Keywords: Cooling, knee, isokinetic dynamometry, performance, sport injury

1 1. Introduction

² It is commonplace within sport to see ice being ap-³ plied at varying times throughout competition to en-

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able the continuation of competitive play. Aetiologi-

cal risk factors strongly associated with non-contact 5 musculoskeletal injury at the knee include reductions 6 in strength [1-3]. Research has detailed the immediate 7 detrimental effect icing protocols may have on muscle 8 strength [4,5] and knee joint kinematics [6,7]. These 9 detrimental effects being shown to exist for > 20-min 10 post application [5,6]. Evidencing that during competi-11 tion, such as half-time, consideration needs to be given 12 to the potential injury risk exposure an athlete may be 13 subjected to post ice application. This provides sports 14

^{*}Corresponding author: Jill Alexander, Sport, Nutrition and Clinical Sciences, School of Sport and Health Sciences, University of Central Lancashire, Preston, UK. Tel.: +44 1772 892781; E-mail: JAlexander3@uclan.ac.uk.

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medicine practitioners with the dilemma of immedi-15 ate therapeutic advantages, against potential increased 16 or further injury risk. Contemporary pneumatic cryo-17 compression devices aim to replicate similar reduced 18 skin surface temperatures (T_{sk}) of between 10–15°C, 19 such as those induced by wetted ice (WI) [8], and al-20 though investigations into technological advances in 21 cooling devices are acknowledged [9], the effects of 22 such modalities on biomechanical function are limited 23 within the available literature. 24 Historically, literature compares traditional cooling 25 modalities such as gel packs, cold spray, crushed ice, 26 frozen peas and WI [10–12]. Although, modern de-27 vices that combine cooling capabilities in conjunction 28 with compression, such as the GameReady[®] (GR), 29 Squid Go[®] and AIRCAST[®] Cryo/Cuff have gained 30 prominence in the literature [8,13–15]. Evidence con-31 siders the addition of compression alongside cooling 32 more effective at reducing T_{sk} [13,16], increasing oxy-33 genation within tendons [17] and muscle [13], and the 34 magnitude of cooling [13,18], compared to the ap-35 plication of cooling alone. The comparison of con-36 temporary cryo-compressive modalilties with intermit-37 tent vs consistent pressure demonstrated equivalent 38 intramuscular temperatures decreases during applica-39 tions [15], interestingly differences in T_{sk} were re-40 ported between modalities [15]. Similar findings are 41 recently reported [13] for T_{sk} following varying lev-42 els of pressure and considered to be a key mecha-43 nism response for physiological processes to occur. 44 Despite the known impact on physiological measures 45 that additional compression influences, studies are still 46 negligible that compare contemporary cooling devices 47 with compression capabilities on strength parameters. 48 This is most likely due to the lack of consensus indi-49

vidually for optimal cryotherapy or compression, in-50 cluding the length of application (minutes), which in-51 forms the rationale for the combined therapeutic use 52 of cryo-compressive devices. Consequently, agreement 53 as to what may be the 'optimum' application of such 54 cryo-compressive devices are not yet determined. Con-55 temporary developments in electronic pneumatic cryo-56 compressive devices include Swellaway® (SA) (Swell-57 away.com), claimed to be a targeted local cooling de-58 vice, and the GR (GameReady.co.uk), which provides 59 intermittent compression with circumferential cooling. 60 Physiological measures of T_{sk} through infrared ther-61 mography (IRT) and functional strength quantifications 62 of the lower limb musculature, via isokinetic dynamom-63 etry (IKD) support the understanding of potential ef-64 fects local cryotherapy may have on objective mark-65

ers of function [5,18,19]. The relationship between re-66 duction of T_{sk} and intramuscular temperature (T_{im}) is 67 previously reported [11], with a suggested quadratic 68 relationship aiding to the understanding of the potential 69 strength changes as reported in some studies following 70 local cryotherapy applications [5,10,19,20]. Varying 71 metrics have been utilised within literature to quantify 72 muscle strength, including peak moment (PM) [1,3,5]. 73 Utilisation of PM metrics provides practitioners with 74 an overview of the athletes peak strength within one 75 degree of movement. The effects of icing on biome-76 chanical function are evident, yet not fully understood 77 in relation to PM when comparing multiple cooling 78 modalities. Methodologies differ however in the loca-79 tion of cooling application on mechanical properties 80 of muscle and strength responses, with some studies 81 applying only distal joint cooling [21,22], and others di-82 rectly over soft tissue structures [23]. Recent literature 83 reported that regardless of cooling location (quadriceps 84 vs knee joint cooling) concentric muscle strength of 85 the quadriceps decreased after exposure to WI applica-86 tion [5]. Further understanding however of contempo-87 rary cryo-compressive devices such as the SA and GR 88 and their effects on biomechanical mechanisms, may 89 support the progression of evidence necessary in help-90 ing to define optimum cryotherapy protocols for sports 91 injury rehabilitation and recovery. Therefore, the aim 92 of the present study is to compare the effect of cooling 93 through the applications of WI, SA and GR on T_{sk} and 94 the PM. 95

2. Methods

2.1. Participants

A priori power calculation was conducted using fa-98 miliarisation trials and a minimum sample size of ≥ 10 99 participants was required to evaluate the interactions 100 associated with all independent variables (for statisti-101 cal power > 0.8; P = < 0.05). The study was adver-102 tised through the University of Central Lancashire, and 103 those volunteers that met the inclusion criteria of play-104 ing semi-professional rugby (classified as National 1 105 or 2 for the purpose of this study) with weekly train-106 ing and competitive fixtures, alongside their univer-107 sity sports commitments were recruited. Consequently 108 eleven healthy male participants met the criterion and 109 volunteered to take part in the study (age: 23 ± 14 years; 110 weight: 78.3 ± 14.5 Kg; height: 180 ± 9.5 cm; body fat: 111 $22.1 \pm 4.7\%$). All experiments were undertaken with 112

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		Time point		
		Pre-intervention	Immediately post intervention	20 minutes post intervention
Wetted Ice				
	T_{sk} (°C)	$28.6\pm0.66^\circ\mathrm{C}$	$6.9 \pm 2.67^{\circ} C^{*}$	$19.7 \pm 1.24^{\circ}C^{*}$
Speed (°s ⁻¹)	$60^{\circ}.s^{-1}$ PM	241.2 ± 54.5	$181.9\pm54.2^\dagger$	$203.2\pm67.6^\dagger$
	$180^{\circ}.s^{-1}$ PM	123.9 ± 39.7	$77.8\pm21.9^{\dagger}$	$110.7\pm33.8^\dagger$
Game ready [®]				
	T_{sk} (°C)	$28.6\pm0.66^\circ C$	$18.4 \pm 2.14^{\circ}C^{*}$	$24.7 \pm 1.46^{\circ}C^{*}$
Speed ($^{\circ}s^{-1}$)	$60^{\circ}.s^{-1}$ PM	199.5 ± 54.5	$175.4\pm69.3^\dagger$	216.5 ± 53.9
	$180^{\circ}.s^{-1}$ PM	147.5 ± 26.8	$112.4\pm35.1^\dagger$	147.7 ± 29.5
Swellaway®				
	T_{sk} (°C) (Medial knee)	$28.6\pm0.66^\circ\mathrm{C}$	$13.4 \pm 1.61^{\circ}C^{*}$	$24.9 \pm 1.78^{\circ}C^{*}$
	T_{sk} (°C) (Lateral knee)	$28.6\pm0.66^\circ C$	$15.0 \pm 2.13^{\circ}C^{*}$	$26.7 \pm 1.69^{\circ}C^{*}$
Speed ($^{\circ}s^{-1}$)	$60^{\circ}.s^{-1}$ PM	204.2 ± 51.1	$148.4\pm35.6^\dagger$	224.9 ± 54.7
	$180^{\circ}.s^{-1}$ PM	141.0 ± 31.9	$103.9\pm34.4^\dagger$	126.2 ± 39.5

*Statistically significant reduction in T_{sk} post intervention. [†]Statistically significant reduction in concentric strength post intervention.

the understanding and written consent of each subject, 113 and the study conformed with The Code of Ethics of the 114 World Medical Association (Declaration of Helsinki, 115 2013), approved by the host university ethics committee 116 (STEMH: approval date: September 2019). All male 117 participation increased sample homogeneity due to gen-118 der differences found in response to local cooling [24]. 119 Criteria for exclusion from this study included; females; 120 any male under 18 years, history of musculoskeletal or 121 neuromuscular lower limb injury in previous 6 months, 122 any contraindications to cryotherapy [7,25]. All data 123 was collected at pre-intervention, immediately post-124 intervention and at 20-min post-intervention. 125

Participants were randomly assigned (randomiza-126 tion.com) to a sequence of cryotherapy modalities, 127 separated by 1 week, which included the GR 128 (GameReady[®], Global, UK), which provides cycli-129 cal pneumatic cooling through water and ice with 130 simultaneous compression through manual protocol 131 combinations; SA (Swellaway Ltd, UK) a pneumatic 132 portable device providing simulataneous targeted cool-133 ing through Peltier cell technology and compression 134 through pre-set protocol combinations; and WI made 135 up from comprised of 800 g of crushed ice mixed with 136 800 ml of water. Each modality followed a typical 137 clinical application times of 15-min dosage [26], stan-138 dardising common practices of cryotherapy applica-139 tions in sport. Anthropometric data, including skin fold 140 measurements (Harpenden Skinfold Callipers, HSB-BI; 141 Baty International, Burgess Hill, West Sussex, UK), 142 to estimate the percentage body fat based on the sum 143 of skin fold thickness for adipose tissue measurements 144 and were taken from the following sites: abdomen, me-145

dial calf, thigh, biceps, triceps, iliac crest, supraspinatus 146 and subscapularis [27]. Records of dominant limb was 147 quantified following previous published methods to de-148 termine favoured kicking foot [28] and ambient room 149 temperature established during a 15-min acclimatisa-150 tion period ensured continuity between baseline data 151 protocols and participants prior to cooling intervention 152 following previous methods [29]. Room temperature 153 measured every 30-min throughout testing noted any 154 fluctuations in environmental temperature. 155

2.2. Testing protocol

Skin surface temperature via a non-invasive thermal 157 imaging camera (FLIR C3, FLIR® Systems, Inc.) and 158 concentric isokinetic quadriceps strength (Cybex, Di-159 vision of Lumex Inc., Ronkonkoma, NY, USA) estab-160 lished relevant objective biomechanical and physiologi-161 cal markers for the study. An accurate and reliable mea-162 sure of T_{sk} can be quantified through thermal imag-163 ing [20,29], and in the current study this provided the 164 opportunity to determine whether differences in T_{sk} 165 exist between the three modalities when applying the 166 same length of exposure (15-min) (Table 1). A Thermo-167 Vision A40M Thermal Imaging Camera (Flir systems, 168 Danderyd, Sweden) with emissivity set at 0.97-0.98 169 was used according to standard medical protocols for 170 the use of Thermographic Imaging in Sport and Exer-171 cise Medicine (TISEM) [29]. Mounted perpendicular 172 to the defined region of interest (ROI) over the ante-173 rior, medial and lateral aspects of the knee, on a tripod 174 at height 53 cm; the TI camera connected to a laptop 175 running Thermacam Researcher Pro 2.8 software (Flir 176

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systems, Danderyd, Sweden). To define the ROI over 177 the knee, thermally inert markers developed a suitable 178 framework for each modality application. Markers to 179 define a ROI for WI and GR applications were placed at 180 the tibial tuberosity, lateral and medial border of patella 181 at the same level with the tibiofemoral joint line, mid-182 dle of the base of the patella [12]. Markers to define 183 a ROI for SA were placed at tibial tuberosity, lateral 184 and medial border of patella at the same level with the 185 tibiofemoral joint line, medial and lateral epicondyles 186 of the femur, and the medial and lateral condyles of 187 the tibia. Three images were taken at each timepoint 188 (Pre; Immediately post intervention; 20-min post in-189 tervention) for each modality, with mean \pm SD T_{sk} 190 established during analysis. 191

The dynamometer was calibrated prior to each test-192 ing session. The data was collected at the same time-193 points of baseline, immediately post intervention and 194 20-min post intervention and achieved by subjects per-195 forming five repetitions of knee extension at 60 and 196 180°/s on the dominant leg [22]. For each testing speed 197 the gravity-corrected moment angle curve was anal-198 ysed. Analysis was restricted to the isokinetic phase 199 with angular sectors of 100° of knee flexion and 0° 200 to extension and for each phase the PM was identi-201 fied. Highest PM values from repetitions for each time-202 point were utilised for analysis. The limb was passively 203 moved into flexion at 10° /s between repetitions with 60 204 second rest between the two sets. Participants received 205 verbal encouragement during the strength assessments. 206 Participant position was supported at the distal thigh, 207 distal tibia and across the chest when seated on the IKD 208 follows standard protocol for this measurement [30]. 209 A 90° hip and knee flexion position prior to the com-210 mencement of movement permitted the input axis of the 211 dynamometer to align with the lateral femoral condyle 212 of the testing limb. Positional settings were recorded 213 for each participant to ensure standardisation between 214 each timepoint of data capture and between the different 215 modality exposures. Throughout testing each repetition 216 was observed by the same researcher to ensure smooth 217 effort was exerted by each participant [22]. 218

Interventions were allocated to participants in a ran-219 dom order of exposure comprised of either the GR; 220 applied over the knee via the anatomical lower limb 221 wrap, set at intermittent high compression (5–75 mm 222 Hg) of 3-minute inflation compression cycles followed 223 by 1-minute recovery deflation, with a target temper-224 ature manually set to 10°C target temperature on the 225 device (Fig. 1); WI comprised of 800 g of crushed ice 226 mixed with 800 ml of water in a sealed bag, held in 227



Fig. 1. Contemporary cryotherapy cooling modalities used in the study; the Game Ready ${}^{\textcircled{R}}$ and the Swellaway ${}^{\textcircled{R}}$ device.

place using standard cling wrap [10] over the anterior 228 aspect of the knee; or the SA knee unit with \times 2 modu-229 lar Peltier cells arranged medially and laterally over the 230 knee joint line, held in place by a custom knee brace, 231 with consistent pressure set at 35 mm Hg and target 232 temperature manually set to 10°C (Fig. 1). All cooling 233 applications were applied with a standardised duration 234 of 15-min [26]. Participants remained in a long sitting 235 position on a medical plinth for the application of each 236 cryotherapy modality. Following immediate removal of 237 the intervention, thermographic images of the anterior 238 knee and concentric quadriceps strength measures were 239 taken following the same protocol as pre-intervention. 240 The participant then returned to a long sitting position 241 for a re-warming period of 20-min before further T_{sk} 242 and the isokinetic moment measurements of the quadri-243 ceps were repeated. The choice to test at 0 and 20-min 244 post-intervention was thought to replicate shorter time 245 periods where athletes may return to functional compet-246 itive activity after exposure to cooling and timepoints 247 representing previously published methodologies [5,7]. 248 During the rewarming period, participants were encour-249 aged to remain as still in the same position through-250 out this time. Participants returned at 1 and 2 weeks 251 via randomisation for exposure to all modalities in the 252 study. 253

2.3. Analysis

Statistical analysis was completed using PASW Statistics Editor 26.0 for Windows (SPSS Inc, Chicago, IL). A univariate, repeated-measures general linear

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model quantified the main effects for recovery duration 258 following cooling interventions and for all isokinetic 259 testing speeds. Significant main effects in recovery du-260 ration were explored using post-hoc pairwise compar-261 isons with a Bonferroni correction applied. To ensure 262 model adequacy the assumptions associated with the 263 statistical model were assessed and met. Mauchly test 264 of sphericity was also completed for all dependent vari-265 ables, with a Greenhouse-Geisser correction applied if 266 the test was significant. To estimate effect sizes for all 267 significant main effects partial eta-squared ($\eta^2 p$) values 268 were calculated and classified as small (0.01–0.059), 269 moderate (0.06-0.137), and large (> 0.138) [31]. Inter-270 actions within the general linear model were identified 271 within the analysis of data. Statistical significance was 272 set at $P \leq 0.05$, and all data are presented as mean 273 (SD). 274

275 **3. Results**

276 3.1. Skin surface temperature (T_{sk})

277Skin surface temperature demonstrated statistically278significant reductions immediately post cooling (P <2790.05) and at 20-min post cooling for all three modalities280(P < 0.05) compared to pre-application temperatures281(Table 1). It did not return to baseline temperatures at28220-min post intervention for any of the three modalities283(Table 1).

284 3.2. Peak moment

Table 1 summarises the effects of all cryotherapy 285 modalities and the temporal pattern of recovery on PM. 286 There was a significant main effect for speed post-287 intervention ($P \leqslant 0.001$, $\eta^2 = 0.47$) and time ($P \leqslant$ 288 0.001, $\eta^2 = 0.21$), with no significant effect of modality 289 found (P > 0.05, $\eta^2 = 0.02$). No significant 2-way or 290 3-way interactions between the variables speed, time 291 and modality were observed (P > 0.05) and there-292 fore led to the examination of modalities separately for 293 further exploration. 294

With the data set separated to consider effects of speed and time for each modality, significant main effects for time and speed for PM were identified for all three modalities (WI: time: P = 0.007, $\eta^2 = 0.17$, speed: $P \le 0.001$, $\eta^2 = 0.546$; GR: time: $P \le 0.001$, $\eta^2 = 0.17$, speed: $P \le 0.001$, $\eta^2 = 0.39$; SA: time: $P \le 0.001$, $\eta^2 = 0.30$, speed: $P \le 0.001$, $\eta^2 = 0.47$).

³⁰² No significant speed x time interaction were found

(P > 0.05) for PM. All modalities identified a significant reduction in strength immediately post intervention (P < 0.05), with only WI however demonstrating a significant reduction in strength 20-min post intervention (P < 0.05) for PM.

3.3. Collapse of test speeds

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Analysis of the different speeds identified significant 309 main effects for time (P < 0.001), but not for modality 310 (P > 0.05) for 60°/s and both time and modality for 311 180° /s (P < 0.001) for PM. Observation of time points 312 for PM for both speeds identified significant differences 313 between time points pre and immediately post interven-314 tion (P < 0.001) and immediately post intervention and 315 20-min post intervention (P < 0.001). Further analysis 316 identified no significant differences in strength at 60°/s 317 between modalities for PM. Strength at 180°/s however 318 identified significant differences between WI and GR 319 (P < 0.001); WI and SA (P < 0.001); but not between 320 GR and SA (P > 0.05). 321

4. Discussion

The purpose of the study was to investigate the effects 323 of three different cryotherapy modalities on concen-324 tric knee extensor strength over a re-warming period. 325 Findings report significant differences in the amount of 326 PM output between GR, SA and WI modalities when 327 applied to the knee for the same exposure period of 15-328 min. With WI having the greatest effect on strength re-329 duction across multiple time points. Optimal cryother-330 apy protocols in sporting contexts are yet to be estab-331 lished. In consideration of the known immediate and la-332 tent effects on strength, a key aetiological risk factor as-333 sociated with non-contact musculoskeletal injury [1-3], 334 it is important to investigate and compare the biome-335 chanical responses across different cryotherapy modal-336 ities to help best inform practical application in sport. 337 This is the first study to the authors knowledge that 338 compares contemporary cryo-compressive devices of-339 fering circumferentical or targeted applications to tra-340 ditional WI methods. Results within the present study 341 are largely consistent with previous work, displaying 342 reductions within strength parameters immediately [5] 343 and up to 20-min post cooling [22]. Yet, findings sug-344 gest the effects may be influenced through choice of 345 cooling modality. 346

It was found that WI had the greatest effect on strength and for a longer period compared to the GR 348

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or SA devices, with significant reductions identified 349 immediately and at 20-min post-intervention. Inter-350 estingly, when observing the two contemporary cryo-351 compressive modalities utilised in this study (GR/SA) 352 they were both associated with significant knee exten-353 sion strength reductions immediately, but not at 20-min, 354 post-intervention. It is evidenced that intramuscular 355 temperatures continue to decrease after removal of cool-356 ing [10,11]. We might assume therefore that due to the 357 efficacy of WI to conduct thermal energy this resulted 358 in the significant reduction of strength at 20-min in the 359 current study. A disruption to neuromuscular response 360 through joint cooling previously suggests this may be a 361 contributing factor to muscle strength loss in surround-362 ing tissues such as the quadriceps [22]. Current data is 363 representative of these presumptions and suggests that 364 different neuromuscular responses occurred between 365 modalities. Known physiological changes that ensue 366 when the apeutic range is met, such as a reduction in 367 nerve conduction velocity which influences joint recep-368 tor feedback [32] may not have been affected at 20-min 369 post GR or SA applications. It is thought that this may 370 be due to a) inadequate length of application exposure 371 (time) to initiate response, and b) smaller, targeted re-372 gion of joint cooling of the SA device compared to WI. 373 The authors acknowledge literature that suggests ex-374 posure (time) should be ideally altered in consideration 375 of adipose tissue levels [8] or target tissue [33] to in-376 duce physiological responses. In the current study however the same length of exposure (15-min) was applied 378 across all particiants and between modalities to ensure 379 standardisation of that particular variable, and was not 380 the main focus of investigation in this study. Contrast-381 ing characteristics between modalities and the phase-382 change capability of material may advocate the results 383 reported and contribute to the differences in strength 384 output. Consequently this has implications on modality 385 choice in terms of therapeutic treatment target. 386

Significant effects were observed in the current study 387 for the speed of test, challenging findings in previous 388 work questioning the use of a variety of speeds within 389 research [34,35]. It is considered that higher velocity 390 speeds more closely reflect the functional demands of 391 multidirectional movements which require increased 392 control at the knee to perform. Furthermore, injury risk 393 is heighted through functional movements performed at 394 higher velocity speeds. In the current study, at speeds of 395 180°/s, significant effects on PM for time and modality 396 compared to only time for the lower speed of 60° /s were 397 reported. Reductions of strength noted at higher speeds 398 compared to lower speed following the application of 399

local knee joint cooling may suggest greater implica-400 tions on functional control exist when observing PM 401 parameters, and be influenced by modality choice. This 402 requires further investigation, however practitioners 403 might consider choice of cooling modality and length 404 of rewarming periods to help mitigate the effects on 405 functional control at the knee following local cooling applications.

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Across all three modalities a typical re-warming 408 curve in T_{sk} was noted, replicating earlier litera-409 ture [25], with T_{sk} having not returned to baseline mea-410 sures at 20-min post-intervention. When comparing de-411 vices on their ability to reduce T_{sk} differences were 412 noted, and may therefore rationalise the differences in 413 muscle strength changes observed in the current study. 414 Notably T_{sk} reductions were significantly greater for 415 WI compared to the GR or SA devices. In line with 416 previous research, it is assumed from the reduction in 417 strength at 20-min post removal of WI, intramuscular 418 temperatures were more adversely affected compared 419 to the GR or SA applications, of the same length of 420 exposure (15-min). Current findings are representative 421 of previous work that suggests that a quadratic relation-422 ship may exist between T_{sk} and T_{im} post cooling [10] 423 and that reductions in intra-articular temperatures may 424 continue after the removal of cooling [36]. Although 425 this is only an assumption as intra-articular tempera-426 ture measures were not in the current study. Consid-427 ering the continuing reductions possible in the intra-428 articular knee joint following removel of such cooling 429 devices and applications; with therapeutic advantages 430 of maintaining tissue temperature reductions, comes 431 the increased potential for risk of further injury through 432 reduced joint control, due to detrimental responses in 433 surrounding muscle strength and meuromuscular re-434 sponses to cooling [5,22]. WI cooled T_{sk} to a lower 435 temperature, over a larger area compared to the SA de-436 vice and as a result unsurprisingly negatively affected 437 strength for a prolonged period post removal. The tar-438 geted cooling application of the SA device demon-439 strated the ability to reduce a local region of T_{sk} that 440 was in direct contact with the Peltier cell, to within the 441 therapeutic range (10–15°C) [25] without diminishing 442 PM 20-min post-application removal. It is important to 443 note that a much smaller targeted area of cooling via the 444 SA device may only be achieved without any indication 445 of cooling spread in the adjacent skin away from the 446 Peltier cell contact, in comparison to the other modali-447 ties, with cooling targeted over medial and lateral knee 448 joint lines in the current study protocol. Although T_{sk} 449 varied between medial and lateral locations (Table 1), 450

 T_{sk} reduced to within the rapeutic range (10–15°C) over 451 both contact areas (medial and lateral knee joint lines) 452 via Peltier cells, the cooling mechanism behind the SA 453 device. This may be beneficial for targeted intervention 454 applications, as no spread of cooling outside Peltier cell 455 skin contact occurs, however as a result circumferen-456 tial cooling cannot be achieved in comparison to the 457 other modalities such as the GR or WI bags. There-458 fore the aim of treatment is important to identify prior 459 to application of cooling modality choice. The rapid 460 re-warming of T_{sk} observed by the SA modality may 461 be advantageous in the development of identifying pa-462 rameters of safer return to activity post cooling, as no 463 detrimental muscle strength losses were reported at 20-464 min post. It may be beneficial however to determine the 465 effects of such device on joint kinematics, perception of 466 pain and other physiological mechanisms to strengthen 467 or dispute these findings further. 468

The 15-min exposure time application and target tem-469 perature setting of 10°C applied in the current study, 470 reflecting pitch side or recovery applications of cool-471 ing appeared inadequate for the GR device to achieve 472 a typical T_{sk} range of between 10–15°C immediately 473 post removal (Table 1). Previous evidence demonstrates 474 the ability of this device to cool to within therapeu-475 tic range [20] yet methodological differences in target 476 temperature between studies as a rationale for the duif-477 ferences, appear to differentiate between agreement in 478 results, which is unsurprising. 479

Despite similar presentations in strength responses 480 for GR and SA devices at 20-min post it is assumed 481 unlikely that detrimental changes in muscle strength 482 would be reported for the GR. Previous literature ap-483 plied an exposure time of 30-min for the GR de-484 vice [14], but the authors felt this was not represen-485 tative of shorter exposures of cryotherapy utilised in 486 sport pitch-side, at half-time or intermittent stoppages in 487 play, hoped to be investigated in the current study. The 488 shorter application time for the GR device in the current 489 study, reduced the capability of comparison to previous 490 methodologies limiting evaluation of outcomes mea-491 sured in the current study to others. Future investiga-492 tions might observe longer periods of applications or 493 cooler target temperatures for the GR (\sim 30 min) as represented in manufacturers' protocol options. This 495 would aid as a dosage comparison and to ensure physi-496 ological changes, notably in analgesia are sufficiently 497 induced. That said, the current findings highlight im-498 portant differences in strength responses that therefore 499 occur between cooling modalities of the same length of 500 exposure (time). Current results suggest that both ben-501

eficial and disadvantageous differences arise between modalities, however as to which modality represents best practice is determined upon the aim of treatment and justification of use within the applied sport setting.

One application difference between the modalities in 506 the current study was the adjunct of compression, that 507 being manual-consistent pressure offered with WI (via 508 plastic wrap), pneumatic-consistent pressure for the SA 509 device, and pneumatic-intermittent pressure of the GR. 510 Furthermore, the level of compression was not quan-511 tified and may be a limitation in the ability to justify 512 the outcomes of the findings. It may be possible that 513 the results of the GR were in fact due to the differences 514 in compression adjunct (in term of intermittent vs con-515 sistent pressure) given that previous literature suggests 516 it can produce similar levels of cooling compared to 517 other cooling modalities [14,20]. Direct comparison 518 to earlier studies is difficult due to differences in the 519 modalities investigated. Further exploration of different 520 methods of compression adjuncts offered by contempo-521 rary cooling modalities is warranted to understand the 522 full extent of the impact it may have on physiological 523 and biomechanical responses. 524

Choice of cryotherapy modality is an important part 525 of clinical decision making. The phase-change capa-526 bility of modalities is of note when comparing the effi-527 cacy of cryotherapeutic modalities, a panacea of vari-528 ables influences this, including metabolic changes asso-529 ciated with injury, modality temperature and compres-530 sive adjunct, alongside length of exposure (time). Fu-531 ture research should consider the differences in material 532 properties and length of exposure (time) of contempo-533 rary cooling applications on biomechanical functions. 534 Subsequently the addition of eccentric muscle strength 535 and joint position sense measures may be beneficial to 536 develop a body of evidence around optimal protocols 537 of contemporary cooling applications in sport. Sports 538 medicine and performance practitioners should however 539 continue to consider the differences and deleterious ef-540 fects some applications of cooling may have on strength 541 following lower limb cooling. A reduction in muscle 542 strength and consequently performance suggests joint 543 stability feedback mechanisms could also be compro-544 mised, as reported in previous literature [5,6]. There-545 fore, contemporary cooling devices that offer targeted 546 local cooling, such as the SA device may be useful in 547 comparison to circumferential joint cooling (GR) and 548 vice versa, dependent on injury presentation, rehabilita-549 tion or recovery aim. The findings of the study are qual-550 ified by the homogeneous sample which limit the trans-551 ferability of findings to female or injured populations. 552

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Further research is required to address this issue and to
 provide sports medicine practitioners with evidenced
 based rationale for application of such modalities.

556 *4.1.* Conclusion and practical implications

Thermal imaging assessment for T_{sk} aided by isoki-557 netic dynamometry continues to advance the devel-558 opment of applied guidelines for cryotherapy. Overall 559 results are an important indication of the variation in 560 effects on muscle strength response for several con-561 temporary and traditional cryotherapeutic modalities. 562 The results highlight the importance of acknowledging 563 strength loss differences that occur between modalities 564 following lower limb knee joint cooling. Precaution 565 for athletes returning to functional activity following 566 cryotherapy is required, and the extent of which is de-567 pendent on several biomechanical factors in need of fur-568 ther investigation simultaneously. Therapists may con-569 sider the following points when applying this modality: 570

 The effects of GameReady[®], Swellaway[®] and wetted ice on muscle strength measures and skin surface temperature observed over a rewarming period differ despite consistent length of exposure (time) applied (15-min).

 Contemporary cooling devices offering circumferential joint cooling (GameReady[®]) may be useful in comparison to targeted local cooling (Swellaway[®]) and vice versa, dependent on the aim of treatment.

 Targeted treatment using the Swellaway[®] device may minimise any deferred deleterious effects of cooling on specific muscle strength parameters.

 Further investigation is required to optimise application protocols using contemporary cooling devices compared to traditional methods for sport injury and recovery strategies.

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591 Author contributions

- 592 CONCEPTION: Jill Alexander, James Selfe, Olivia
- ⁵⁹³ Greenhalgh and David Rhodes
- ⁵⁹⁴ PERFORMANCE OF WORK: Jill Alexander, Olivia
- ⁵⁹⁵ Greenhalgh and David Rhodes

INTERPRETATION OR ANALYSIS OF DATA: Jill Alexander, James Selfe, Olivia Greenhalgh and David Rhodes PREPARATION OF THE MANUSCRIPT: Jill Alexander, James Selfe, Olivia Greenhalgh and David Rhodes REVISION FOR IMPORTANT INTELLECTUAL CONTENT: Jill Alexander, James Selfe, Olivia Greenhalgh and David Rhodes SUPERVISION: James Selfe and David Rhodes

Ethical considerations

All experiments were undertaken with the understanding and written consent of each subject, and the study conformed with The Code of Ethics of the World Medical Association (Declaration of Helsinki, 2013), approved by the University of Central Lancashire ethics committee (STEMH: approval date: September 2019).

Conflict of interest		
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