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1 **The effect of a modified elastic band orthosis on gait and balance in stroke**  
2 **survivors**

3 Thitithunwarat N, Krityakiarana W, Kheowsri S, Jongkamonwiwat N, Richards J.

4 **Abstract**

5 **Introduction:** Gait is crucial for independent living for stroke survivors and assistive devices  
6 have been developed to support gait performance. Ankle foot orthoses (AFOs) are commonly  
7 provided to stroke survivors to prevent foot drop during walking. However, previous studies  
8 have reported limitations of AFOs including them being too heavy, creating skin irritation, and  
9 being a stigma of disability. The purpose was to compare the gait and balance improvement  
10 between elastic band orthoses (EBOs) and AFOs.

11 **Materials and Methods:** The AFOs and EBOs were provided to 17 stroke survivors, and  
12 changes in gait and balance were assessed compared to barefoot (control). Gait  
13 spatiotemporal parameters were measured using the zebris-FDM-Rehawalk® system, and  
14 balance ability was evaluated using the timed up and go test (TUG). Satisfaction with the  
15 EBOs was determined using the Quebec user evaluation of satisfaction with assistive  
16 technology (QUEST2.0) questionnaire.

17 **Results:** The EBO showed significant differences in; gait speed, cadence, stride length, stride  
18 time, step length unaffected side, stance phase and swing phase on the affected side, and  
19 pre-swing on the unaffected side, and balance performance (TUG) ( $p < 0.05$ ) when compared  
20 to the AFO and control conditions. The participants were quite satisfied with the EBOs with  
21 QUEST2.0 scores greater than 4 out of 5.

22 **Conclusions:** EBOs could be provided to stroke survivors given their acceptability and  
23 properties to improve gait and balance. The EBO used in this study offered clinically important  
24 improvements in gait and balance when compare to AFO and control conditions, and could  
25 mitigate against some of the limitations reported in the use of AFOs in stroke survivors.

26 **Key words:** elastic band orthoses, ankle foot orthoses, assistive devices, gait, satisfaction.

## 27 **1. Introduction**

28           Stroke is a leading cause of death and disability worldwide. The prevalence of stroke  
29 in Thailand has been reported to be 1.88% in people aged 65 years rising to 2.7% in older  
30 individuals <sup>1</sup>. Stroke often leads to hemiparesis and assistive devices are often provided to  
31 improve activities of daily living. Independent walking is one of the rehabilitation goals for  
32 hemiparetic patients <sup>2,3</sup>. Spasticity is the most common impairment in motor function in stroke  
33 survivors affecting mobility, walking and transfer ability, and can induce an asymmetrical gait  
34 pattern and can contribute to compensatory movement patterns <sup>2,4</sup>. It has been reported that  
35 spasticity of ankle plantar flexors and invertors while walking often occurs, which can disturb  
36 an individual's walking ability in both stance and swing phase of the gait cycle <sup>5,6</sup>. In stance  
37 phase, body weight is often distributed on the lateral border of the affected foot and increases  
38 stance time of the unaffected limb. In swing phase of the affected limb, patients will lean and  
39 shift weight to the unaffected limb resulting in an increased stance phase duration on the  
40 unaffected side. This could cause a loss of balance and lead to falls while walking  
41 independently <sup>6,7</sup>.

42           Applying assistive technology (AT) to stroke survivors follows the Human, Activity,  
43 Assistive Technology (HAAT) model developed by Albert Cook <sup>8,9</sup>, which highlights the  
44 importance of a needs evaluation from key stakeholders when considering the implementation  
45 of AT. Ankle foot orthoses (AFOs) are registered on the national assistive technology list for  
46 persons with disabilities in Thailand. The purpose of AFOs is to assist the patients in regaining  
47 walking ability, preventing foot-drop and the occurrence of toe clearance problems, promoting  
48 ankle stability during standing, and promoting heel strike <sup>10-15</sup>. These have been shown to  
49 increase ground reaction forces in individuals with plantar flexor weakness <sup>16</sup>, however several  
50 studies have reported that AFOs might interfere with a patients' gait performance due to their  
51 weight <sup>10,17</sup>. In long-term use these have been reported to reduce dorsiflexor muscle activation  
52 <sup>18</sup> and have also been shown to interfere with balance in stroke survivors <sup>19</sup>. In addition, when

53 inquiring about the feeling while wearing AFOs, skin irritation and rashes over the contact  
54 areas have been reported <sup>7,10,17,19-21</sup>.

55 Due to these existing limitations, the development of AT for stroke survivors to improve  
56 gait performance continues. Elastic band orthoses (EBOs) have been used to mitigate against  
57 some of the limitations of AFOs, which have been reported to improve balance and gait  
58 parameters in stroke survivors <sup>13,22</sup>, however further studies are required to compare the  
59 effectiveness of EBOs with AFOs before being widely implemented within AT service delivery.  
60 EBOs have been presented in several patents from several countries <sup>13,22,23</sup>. However, to the  
61 authors' knowledge a comparison of EBO with AFO has not been reported. Therefore, the  
62 purpose of this study was to compare balance and gait performance in stroke survivors when  
63 using an EBO and AFO when compared to a control condition, and to determine user  
64 satisfaction with the EBO.

65

## 66 **2. Methods**

### 67 **2.1. Participants**

68 Participants diagnosed with stroke were recruited from the Prasat Neurological  
69 Institute, Bangkok, Thailand. All participants provided informed, written consent prior to  
70 enrollment in the study. The inclusion criteria were; diagnosis of hemiplegia due to  
71 hemorrhagic or ischemic stroke, more than 3 months post-stroke, age over 18 years, spastic  
72 ankle with plantar-flexion and inversion (Modified Ashworth Scale (MAS) 1-3), no shortening  
73 or contracture around the ankle, able to walk more than 10 meters independently with or  
74 without an assistive device, experience of using an AFO, and the ability to understand verbal  
75 instructions. Exclusion criteria were; stroke involving more than one hemisphere, recurrent  
76 stroke, Thai version of the Rowland Universal Dementia Assessment Scale (RUDAS) score  
77 of less than 24 out of 30, and pre-morbid or other musculoskeletal problems affecting gait

78 performance. Ethics approval for this study was approved by the Human Research Ethics  
79 Committee (MU-CIRB 2018/144.1207) and (Ref. number 008/2562).

80

## 81 **2.2. Sample size calculation**

82 The sample size for this study was calculated using G\*Power version 3.1 (G power,  
83 Germany)<sup>24</sup>. Time up and go (TUG) and spatiotemporal parameters were used to calculate  
84 sample size. Based on the data from a pilot study, the estimated sample to obtain a power of  
85 90% with a five percent significance level was 17 participants.

86

## 87 **2.3. Procedures**

88 The researchers explained the protocol to participants and demonstrated walking on  
89 the Force Distribution Measurement/Win FDM device before taking consent. The participants  
90 were asked to walk barefoot (control condition) and whilst wearing an EBO and AFO (with  
91 shoes), the order of which were randomised. The barefoot condition aimed to investigate the  
92 spatiotemporal parameters without any support, and the AFO condition was used as a  
93 reference standard management to compare with the EBO. They were required to walk 10  
94 meters at their most comfortable speed, and were allowed to use an additional walking aid if  
95 needed. Three trials under each condition were performed over a 3 meter walkway, and a 3  
96 minute rest was allowed between trials and a 10 minute rest was allowed between conditions.

97

## 98 **2.4 EBO and AFO interventions**

99 The EBO consisted of an open toe non-slip sock with two straps (Figure 1a, b). The  
100 two different lengths of straps are attached on both sides of the sock. A long strap is placed  
101 on the medial side and goes across the top of the dorsum of the foot to the opposite side  
102 above the lateral malleolus and wraps around the lower leg above the gastrocnemius back to

103 the medial side. The short strap on the lateral side goes across the top of the dorsum of the  
104 foot and wraps across the gastrocnemius back to the lateral side. Both straps are fixed with  
105 Velcro in front of the tibial tuberosity. The AFO was a non-hinged custom-made Polypropylene  
106 Posterior Leaf Spring (Polypropylene PLS), and was chosen and fitted by a qualified  
107 practitioner (physician, PT and Prosthetist) which considered the individual participants clinical  
108 needs (Figure 1c). The protocol and material used in the AFO production was similar for all  
109 participants.

110

## 111 **2.5. Outcome measures**

112 The TUG is a standard test for testing mobility and balance impairment. This test  
113 required participants to stand up, walk 3 meters, make a turn, walk back to the chair, and sit  
114 down. The time was recorded from when their buttocks lifted from the chair to when their  
115 buttocks touched the seat. During the turn the participants were required to turn toward the  
116 unaffected side.

117 Spatiotemporal gait parameters included; velocity, cadence, stride length, step length,  
118 stride time, step time, stance time, single support time, and double support time, which were  
119 recorded on the Zebris FDM Rehawalk<sup>®</sup> system. The walkway consists of an electronic mat  
120 embedded underneath a walkway consisting of 10,240 miniature force sensors, each  
121 approximately 0.85 × 0.85 cm, which recorded the foot placements and timings. The stride  
122 length and step length were normalized by participants' height.

123 The modified Ashworth scale (MAS) is the most widely used clinical scale used to  
124 measure muscle spasticity in the subacute and chronic phases post stroke. The spasticity  
125 according to the MAS (0 = no spasticity, 5 = rigidity), was assessed in the hip adductors, knee  
126 flexors and extensors, ankle plantar flexors and supinators. In addition, the Fugl-Meyer Motor  
127 Assessment-Lower Extremity (FMA-LE) was used to evaluate the motor function. FMA-LE  
128 consists of 17 items, with a maximum possible score of 34 points. Each item was answered

129 using a 3-point ordinal scale (0 = cannot perform, 1 = can partially perform, 2 = can fully  
130 perform). In addition, the Rowland Universal Dementia Assessment Scale (RUDAS)-Thai  
131 version was used to screen cognitive performance. The RUDAS score lower or equal to 23  
132 represents a cognitive function impairment. All assessments were completed by trained  
133 registered physical therapists.

134 The Quebec user evaluation of satisfaction with assistive technology version 2.0  
135 (QUEST 2.0) is a 12-item outcome measure that assesses user satisfaction with the device  
136 (8 items), services (4 items), and open-ended questions. The 8 device items and open-ended  
137 questions were collated to assess user satisfaction of the EBO.

138

## 139 **2.6. Data analysis**

140 The general characteristics of participants were analyzed using descriptive statistics.  
141 Kolmogorov Smirnov tests were used to identify the distribution of the data and all data were  
142 found to be not normally distributed. Friedman tests were performed to determine differences  
143 between the conditions for the affected and unaffected sides separately. Where significant  
144 differences were seen post hoc Wilcoxon-signed rank test were performed to determine  
145 differences between individual conditions for the gait and balance outcome measures. All data  
146 were analyzed using SPSS (IBM, USA), and the alpha level was set at 0.05.

147

## 148 **3. Results**

149 Seventeen individuals (11 males and 6 females) with hemiplegia were recruited. The  
150 mean age was  $50.82 \pm 13.54$  years with a mean body mass index of  $22.86 \pm 2.70$  kg/m<sup>2</sup>. The  
151 participants characteristics are presented in Table 1.

152

### 153 **3.1. Gait and balance measures**

154 Friedman tests revealed significant differences between the three conditions for; stride  
155 length ( $p=0.016$ ), stride time ( $p=0.006$ ), cadence ( $p=0.005$ ), velocity ( $p=0.001$ ), percentage  
156 stance phase on the affected side ( $p=0.025$ ), percentage swing phase on the affected side  
157 ( $p=0.025$ ), step length on the unaffected side ( $p=0.029$ ) and percentage pre-swing phase on  
158 the unaffected side ( $p=0.025$ ). In addition, the TUG test also showed significant differences  
159 between the three conditions ( $p=0.001$ ).

160 Post hoc Wilcoxon Signed Rank test showed differences between the EBO and the  
161 control condition with the EBO showing an increase in stride length ( $p=0.009$ ), percentage  
162 swing phase on the affected side ( $p=0.003$ ), and step length on the unaffected side ( $p=0.035$ ).  
163 Moreover, the EBO showed a decrease in the percentage of stance phase on the affected  
164 side ( $p=0.01$ ), percentage of pre-swing phase on the unaffected side ( $p=0.035$ ), and TUG test  
165 ( $p=0.008$ ). Significant differences were also seen between the EBO and AFO conditions with  
166 the EBO showing a greater stride length ( $p=0.008$ ), cadence ( $p=0.004$ ), velocity ( $p=0.001$ ),  
167 and step length on the unaffected side ( $p=0.031$ ), with a shorter stride time ( $p=0.009$ ) and  
168 TUG test time ( $p=0.001$ ). In addition, the AFO increased velocity ( $p=0.044$ ) when compare to  
169 the control condition. The AFO showed higher TUG test time when compare to control  
170 condition, but it was not significant difference (Table 3, Figure 2-3).

171

### 172 **3.2. User Evaluation of Satisfaction**

173 The QUEST 2.0 and open-ended questions showed that participants were most  
174 satisfied with the weight of the EBO (Median=5, IQR=0) and were least satisfied with the  
175 durability (Median=3, IQR=1) (Table 2). The open ended questions of QUEST showed positive  
176 comments from participants about the EBO associated with the weight and ability to walk  
177 freely, better than the AFO (100%). The participants reported that they wanted to use the EBO  
178 at home in their daily activities (82.4%). However, 17.6% reported they did not want to use the  
179 device with the most common reasons being they needed more time to practice with the EBO,



180 with some participants not wanting to use any assistive device. Additional comments included  
181 that the EBO felt like wearing a pair of socks, which was comfortable and supported firmly at  
182 the ankle, and made the participants feel more confident during walking (100%). They also  
183 perceived that the EBO aided their walking pattern and corrected their posture and helped  
184 their speed (100%). Moreover, they reported that their ankle and toe twitch during walking  
185 were decreased (58.8%).

186

## 187 **4. Discussion**

188         Assistive technology for stroke survivors has been developed for decades. Several  
189 studies have demonstrated that ankle supports can alter gait and balance performance in this  
190 population <sup>7,10-15,17,20,22,23</sup>. Several types of ankle support are available which include ankle foot  
191 orthosis (AFO), which are prescribed to stroke survivors to support their ambulation. However,  
192 the AFO still has some limitations, especially limiting ankle movement during walking <sup>12,17,19,21</sup>.  
193 The purpose of this study was to investigate the effect of an elastic band orthosis on gait and  
194 balance performance in stroke survivors and to provide a comparison with AFOs.

195

### 196 **4.1 Gait and balance performance**

197         Gait and balance performance was assessed through spatiotemporal gait parameters  
198 and the TUG test. Significant differences were found in velocity, cadence, stride length, stride  
199 time, stance phase and swing phase on the affected side, and pre-swing and step length on  
200 the unaffected side, and the TUG test when using the EBO. These findings are in line with  
201 previous studies whereby step length on the unaffected side was improved after applying both  
202 rigid and elastic ankle supports <sup>14,22,25</sup>. However, the EBO significantly improved  
203 spatiotemporal gait parameters when compared with the AFO. This implies that the EBO  
204 encourages weight bearing and gait performance during stance phase on the affected side,  
205 and longer step lengths on the unaffected side. When comparing the two devices the AFO

206 limits the amount of ankle dorsiflexion which affected reaching and gait performance <sup>15,17,26</sup>.  
207 Particularly during stance, limited ankle dorsiflexion in the affected side could lead to a shorter  
208 step length <sup>27</sup>, and stride length in the AFO when compared to the control condition and EBO.  
209 Whereas the EBO offers little restriction of dorsiflexion as this is made from elasticated fabric.

210 The EBO subtly altered the proportions of stance phase and swing phase of the  
211 affected side moving these closer to the normal stance and swing proportions (60:40) when  
212 compared to the control and AFO conditions. The decrease of pre-swing phase on the  
213 unaffected side while walking using the EBO indicated that the transition phase between  
214 stance and swing on the unaffected side was improved. This phenomenon might be related to  
215 improved stability of the affected side during the stance phase, and lead the unaffected side  
216 to become more efficient during propulsion <sup>10,13,14,23</sup>. These affects are associated with force  
217 from the elastic bands within the EBO which provide some supportive properties for the ankle  
218 joint during single limb loading in stance phase on the affected side, and might lead to a longer  
219 step length of the unaffected side. Collectively this led to the improvement in stride time,  
220 cadence, velocity and TUG test time in this sample of stroke survivors. However, the elastic  
221 properties and the optimum force needed for the best function needs to be further explored.

222

#### 223 **4.2. User Evaluation of Satisfaction**

224 The QUEST 2.0 questionnaire was used to evaluate satisfaction with the EBO. The  
225 questionnaire was selected as it has previously been presented to be a valid measure of  
226 satisfaction with assistive devices <sup>28</sup>. Overall, patients were quite satisfied with the EBO  
227 (Median=4, IQR=1). All participants supported that the EBO could be used to improve balance  
228 during walking. It encouraged participants to walk confidently, and their comments seemed to  
229 relate to the findings from the gait and balance performance measures. Compared to the  
230 control condition, the EBO was reported to support the affected ankle in dorsiflexion with  
231 eversion, which promoted patients' ability to clear their toe from the floor and the participants

232 reported that the EBO felt lighter than the AFO. It is noteworthy that polypropylene  
233 development and hybrid AFOs made of polypropylene and fabric have been explore to  
234 facilitate the gait in stroke survivors<sup>28-30</sup>. The lighter weight orthoses showed a higher level of  
235 satisfaction which supports the current findings from the EBO. While the majority of items  
236 showed users were quite satisfied with the EBO (7 out of 8 items), the durability of the EBO  
237 presented as more or less satisfied (1 out of 8 items). Following the concept of the HAAT  
238 (Human, Activity, Assistive Technology) model evaluated by QUEST 2.0, the EBO improved  
239 the gait and balance performance for stroke survivors during walking<sup>8,9</sup>. Participants (82.4%)  
240 agreed that the EBO was suitable for their home environment and wanted to use the EBO in  
241 their daily living. The EBO seems to offer better results than the AFO when considering both  
242 the gait and balance performance and comments from this sample of stroke survivors. A  
243 comparison of the satisfaction when wearing AFOs and EBOs using the QUEST 2.0 might be  
244 considered in further investigations.

245 It has been presented that the Fugl-Meyer score of lower extremity function cut-off  
246 score for high level of mobility function in chronic stroke survivors is 21 out of 35<sup>31</sup>. Using this  
247 score all participants in this current study were deemed to have a high level of mobility function  
248 (Table 1). Further investigation in individuals with different levels of function to further  
249 understand the generalizability of these results is recommended.

250

## 251 **5. Conclusion**

252 The EBO seems to improve TUG, gait velocity, cadence, stride length, stride time,  
253 stance phase and swing phase on the affected side, and pre-swing and step length on the  
254 unaffected side over both the AFO and control conditions, which are reflected by the user  
255 evaluations of satisfaction. Therefore, the EBO could be used in clinical and community  
256 settings, and could mitigate against some of the limitations reported in the use of AFOs in  
257 stroke survivors.

258

259 **Figure 1** The Elastic Band Orthosis (EBO) (The A band contributes the inversion and the B  
260 band contributes the eversion) (a-b) and Polypropylene Posterior Leaf Spring (Polypropylene  
261 PLS) (c)

262

263 **Figure 2** Presented the median (IQR) among three groups (Control, AFO and EBO). The post  
264 hoc Wilcoxon Signed rank test identified the significant difference between pairs.

265

266 **Figure 3** Presented the median (IQR) of stride time (sec) and velocity (km/hr.) among three  
267 groups (Control, AFO and EBO). The post hoc Wilcoxon Signed rank test identified the  
268 significant difference between pairs. (\*  $P < 0.05$ , \*\*  $P < 0.005$ )

269

270 **Table 1** Present the specific conditions and lower limb Modified Ashworth Scale (MAS)

271

272 **Table 2** Present the Quebec User Evaluation of Satisfaction with assistive Technology version  
273 2.0 (QUEST-2.0), Assistive device section, from participants after used EBO

274

275 **Table 3** Present the spatiotemporal parameters and TUG among 3 conditions (Control, AFO  
276 and EBO)

277

278

279

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281

282

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284

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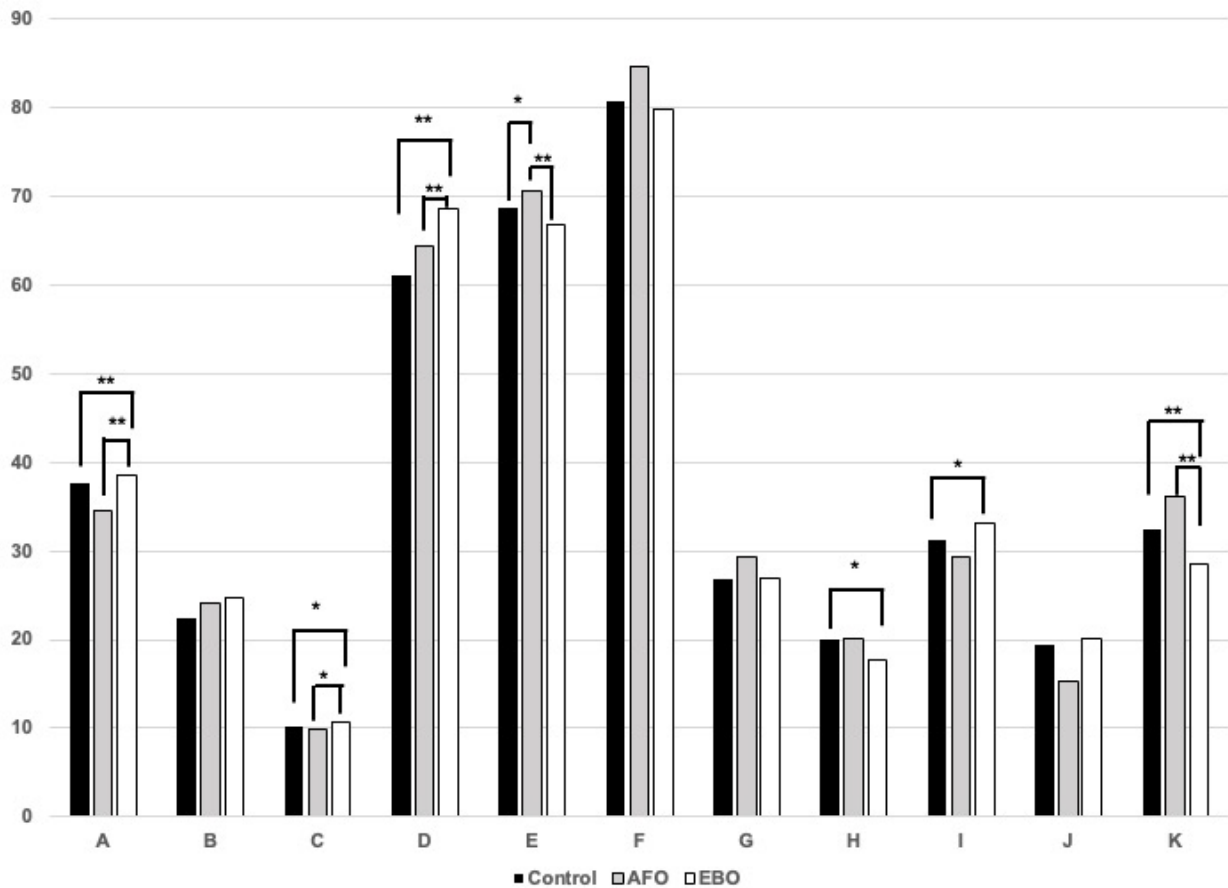
(b)

(c)



388 **Figure 1** The Elastic Band Orthosis (EBO) (The A band contributes the inversion and the B  
389 band contributes the eversion) (a-b) and Polypropylene Posterior Leaf Spring (Polypropylene  
390 PLS) (c)

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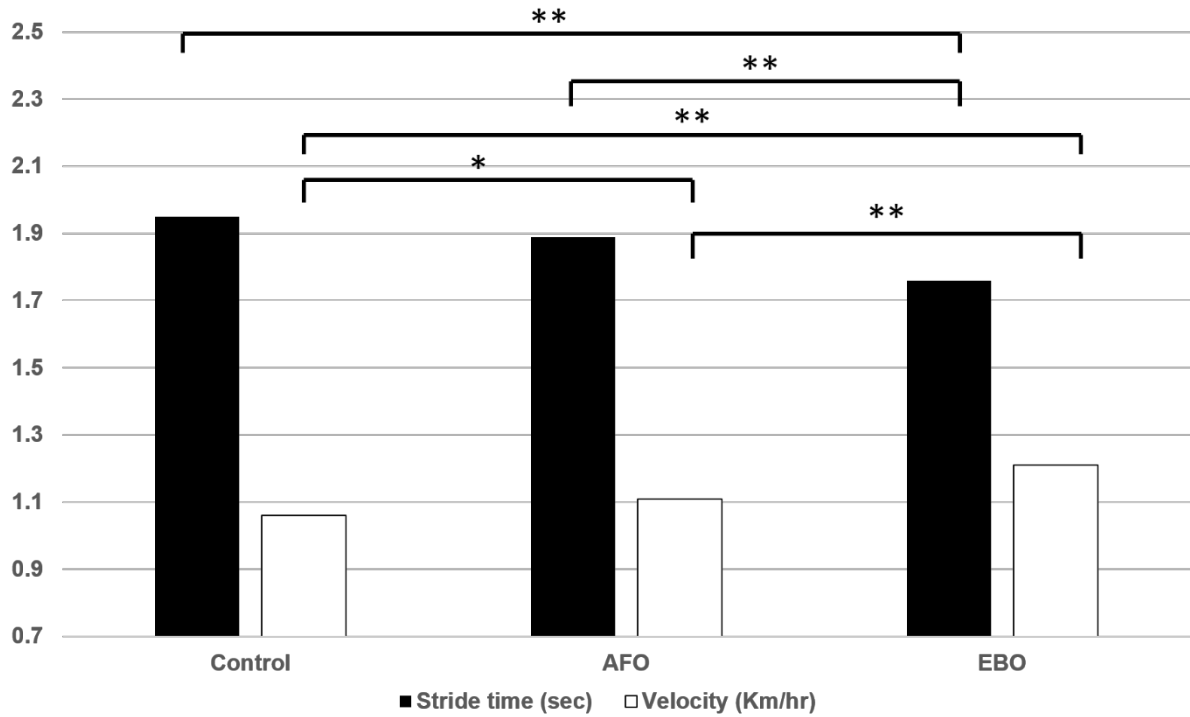
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393 **Figure 2** Presented the median (IQR) among three groups (Control, AFO and EBO). The post  
 394 hoc Wilcoxon Signed rank test identified the significant difference between pairs.

395 (\* P<0.05, \*\* P<0.005, A= Stride length (%), B= Step length affected side (%), C= Step length unaffected  
 396 side (%), D= Cadence (step), E= Stance phase affected side (% gait cycle), F= Stance phase unaffected  
 397 side (% gait cycle), G= Pre-swing phase affected side (%), H= Pre-swing phase unaffected side (%), I=  
 398 Swing phase affected side (%), J= Swing phase unaffected side (%), and K= Time up and go (TUG)  
 399 (seconds))

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403 **Figure 3** Presented the median (IQR) of stride time (sec) and velocity (km/hr.) among three  
 404 groups (Control, AFO and EBO). The post hoc Wilcoxon Signed rank test identified the  
 405 significant difference between pairs. (\* P<0.05, \*\* P<0.005)

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408 **Table 1** Present the specific conditions and lower limb Modified Ashworth Scale (MAS)

Conditions	Mean ± SD	Number	Percent (%)
Diagnosis			
Ischemic stroke		15	88.20
Hemorrhagic stroke		2	11.80
Duration of onset (months)	10.65±16.63		
Affected side			
Left		9	52.90
Right		8	47.10
Modified Ashworth Scale (MAS):			
Ankle planta flexor and supinator		7	41.20
Spasticity Level 1		10	58.80
Spasticity Level 2			
Fugl-Meyer Motor Assessment (FMA)	25.00 ± 3.20		
Lower Extremity) (total = 34)	(Min = 18 - Max = 29)		
Rowland Universal Dementia	29.26 ± 1.28		
Assessment Scale (RUDAS, total 30)	(Min = 25 – Max = 30)		

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411 **Table 2** Present the Quebec User Evaluation of Satisfaction with assistive Technology version

412 2.0 (QUEST-2.0), Assistive device section, from participants after used EBO

QUEST (Version-2.0) Assistive device	Score EBO from participants	
	Median	IQR
1. the dimensions (size, height, length, width) of your assistive device?	5	0.5
2. the weight of your assistive device?	5	0
3. the ease in adjusting (fixing, fastening) the parts of your assistive device?	4	1.5
4. how safe and secure your assistive device is?	4	1
5. the durability (endurance, resistance to wear) of your assistive device?	3	1
6. how easy it is to use your assistive device?	4	1
7. how comfortable your assistive device is?	4	1
8. how effective your assistive device is (the degree to which your device meets your needs)?	4	1
Overall score	4	1

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415 **Table 3** Present the spatiotemporal parameters and TUG among 3 conditions (Control, AFO  
 416 and EBO)

Spatiotemporal gait parameters	Median (IQR)			p-value <sup>a</sup>
	Control	AFO	EBO	
Velocity (km/h)	1.06 (0.99)	1.11 (0.82)	1.21 (0.98)	0.001**
Stride length (%)	37.73 (17.70)	34.64 (15.14)	38.50 (17.75)	0.016*
Step length (%) -Affected side -Unaffected side	22.33 (6.84) 10.27 (11.08)	24.12 (6.97) 9.92 (15.90)	24.64 (11.38) 10.69 (15.27)	0.51 0.029*
Cadence (step/minute)	61.17 (33.20)	64.37 (24.13)	68.62 (27.00)	0.005*
Stride time (sec)	1.95 (1.05)	1.89 (0.78)	1.76 (0.79)	0.006*
Stance phase (% gait cycle) -Affected side -Unaffected side	68.70 (11.75) 80.68 (12.56)	70.66 (12.29) 84.66 (11.62)	66.77 (11.83) 79.88 (11.35)	0.025* 0.33
Pre-swing phase (%) -Affected side -Unaffected side	26.81 (15.54) 20.11 (7.15)	29.34 (13.79) 20.12 (10.51)	26.90 (17.24) 17.8 (7.31)	0.66 0.025*
Swing phase (% gait cycle) -Affected side -Unaffected side	31.30 (11.75) 19.32 (12.56)	29.34 (12.30) 15.34 (11.62)	33.23 (11.82) 20.12 (11.31)	0.025* 0.33
TUG score (seconds)	32.40 (24.23)	36.05 (22.26)	28.60 (23.81)	0.001**

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418 <sup>a</sup> Friedman test, IQR = Interquartile Range, \* P<0.05, \*\* P<0.005

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