

Central Lancashire Online Knowledge (CLoK)

Title	The effect of a modified elastic band orthosis on gait and balance in stroke survivors
Type	Article
URL	https://clock.uclan.ac.uk/45583/
DOI	##doi##
Date	2023
Citation	Thitithunwarat, Nutkrittta, Kritiyakiarana, Warin, Kheowsri, Suchittra, Jongkamonwiwat, Nopporn and Richards, James orcid iconORCID: 0000-0002-4004-3115 (2023) The effect of a modified elastic band orthosis on gait and balance in stroke survivors. Prosthetics & Orthotics International, Publis . ISSN 0309-3646
Creators	Thitithunwarat, Nutkrittta, Kritiyakiarana, Warin, Kheowsri, Suchittra, Jongkamonwiwat, Nopporn and Richards, James

It is advisable to refer to the publisher's version if you intend to cite from the work. ##doi##

For information about Research at UCLan please go to <http://www.uclan.ac.uk/research/>

All outputs in CLoK are protected by Intellectual Property Rights law, including Copyright law. Copyright, IPR and Moral Rights for the works on this site are retained by the individual authors and/or other copyright owners. Terms and conditions for use of this material are defined in the <http://clock.uclan.ac.uk/policies/>

1 **The effect of a modified elastic band orthosis on gait and balance in stroke**
2 **survivors**

3 Thitithunwarat N, Krityakiarana W, Kheowsri S, Jongkamonwiwat N, Richards J.

4 **Abstract**

5 **Introduction:** Gait is crucial for independent living for stroke survivors and assistive devices
6 have been developed to support gait performance. Ankle foot orthoses (AFOs) are commonly
7 provided to stroke survivors to prevent foot drop during walking. However, previous studies
8 have reported limitations of AFOs including them being too heavy, creating skin irritation, and
9 being a stigma of disability. The purpose was to compare the gait and balance improvement
10 between elastic band orthoses (EBOs) and AFOs.

11 **Materials and Methods:** The AFOs and EBOs were provided to 17 stroke survivors, and
12 changes in gait and balance were assessed compared to barefoot (control). Gait
13 spatiotemporal parameters were measured using the zebris-FDM-Rehawalk® system, and
14 balance ability was evaluated using the timed up and go test (TUG). Satisfaction with the
15 EBOs was determined using the Quebec user evaluation of satisfaction with assistive
16 technology (QUEST2.0) questionnaire.

17 **Results:** The EBO showed significant differences in; gait speed, cadence, stride length, stride
18 time, step length unaffected side, stance phase and swing phase on the affected side, and
19 pre-swing on the unaffected side, and balance performance (TUG) ($p < 0.05$) when compared
20 to the AFO and control conditions. The participants were quite satisfied with the EBOs with
21 QUEST2.0 scores greater than 4 out of 5.

22 **Conclusions:** EBOs could be provided to stroke survivors given their acceptability and
23 properties to improve gait and balance. The EBO used in this study offered clinically important
24 improvements in gait and balance when compare to AFO and control conditions, and could
25 mitigate against some of the limitations reported in the use of AFOs in stroke survivors.

26 **Key words:** elastic band orthoses, ankle foot orthoses, assistive devices, gait, satisfaction.

27 **1. Introduction**

28 Stroke is a leading cause of death and disability worldwide. The prevalence of stroke
29 in Thailand has been reported to be 1.88% in people aged 65 years rising to 2.7% in older
30 individuals ¹. Stroke often leads to hemiparesis and assistive devices are often provided to
31 improve activities of daily living. Independent walking is one of the rehabilitation goals for
32 hemiparetic patients ^{2,3}. Spasticity is the most common impairment in motor function in stroke
33 survivors affecting mobility, walking and transfer ability, and can induce an asymmetrical gait
34 pattern and can contribute to compensatory movement patterns ^{2,4}. It has been reported that
35 spasticity of ankle plantar flexors and invertors while walking often occurs, which can disturb
36 an individual's walking ability in both stance and swing phase of the gait cycle ^{5,6}. In stance
37 phase, body weight is often distributed on the lateral border of the affected foot and increases
38 stance time of the unaffected limb. In swing phase of the affected limb, patients will lean and
39 shift weight to the unaffected limb resulting in an increased stance phase duration on the
40 unaffected side. This could cause a loss of balance and lead to falls while walking
41 independently ^{6,7}.

42 Applying assistive technology (AT) to stroke survivors follows the Human, Activity,
43 Assistive Technology (HAAT) model developed by Albert Cook ^{8,9}, which highlights the
44 importance of a needs evaluation from key stakeholders when considering the implementation
45 of AT. Ankle foot orthoses (AFOs) are registered on the national assistive technology list for
46 persons with disabilities in Thailand. The purpose of AFOs is to assist the patients in regaining
47 walking ability, preventing foot-drop and the occurrence of toe clearance problems, promoting
48 ankle stability during standing, and promoting heel strike ¹⁰⁻¹⁵. These have been shown to
49 increase ground reaction forces in individuals with plantar flexor weakness ¹⁶, however several
50 studies have reported that AFOs might interfere with a patients' gait performance due to their
51 weight ^{10,17}. In long-term use these have been reported to reduce dorsiflexor muscle activation
52 ¹⁸ and have also been shown to interfere with balance in stroke survivors ¹⁹. In addition, when

53 inquiring about the feeling while wearing AFOs, skin irritation and rashes over the contact
54 areas have been reported ^{7,10,17,19-21}.

55 Due to these existing limitations, the development of AT for stroke survivors to improve
56 gait performance continues. Elastic band orthoses (EBOs) have been used to mitigate against
57 some of the limitations of AFOs, which have been reported to improve balance and gait
58 parameters in stroke survivors ^{13,22}, however further studies are required to compare the
59 effectiveness of EBOs with AFOs before being widely implemented within AT service delivery.
60 EBOs have been presented in several patents from several countries ^{13,22,23}. However, to the
61 authors' knowledge a comparison of EBO with AFO has not been reported. Therefore, the
62 purpose of this study was to compare balance and gait performance in stroke survivors when
63 using an EBO and AFO when compared to a control condition, and to determine user
64 satisfaction with the EBO.

65

66 **2. Methods**

67 **2.1. Participants**

68 Participants diagnosed with stroke were recruited from the Prasat Neurological
69 Institute, Bangkok, Thailand. All participants provided informed, written consent prior to
70 enrollment in the study. The inclusion criteria were; diagnosis of hemiplegia due to
71 hemorrhagic or ischemic stroke, more than 3 months post-stroke, age over 18 years, spastic
72 ankle with plantar-flexion and inversion (Modified Ashworth Scale (MAS) 1-3), no shortening
73 or contracture around the ankle, able to walk more than 10 meters independently with or
74 without an assistive device, experience of using an AFO, and the ability to understand verbal
75 instructions. Exclusion criteria were; stroke involving more than one hemisphere, recurrent
76 stroke, Thai version of the Rowland Universal Dementia Assessment Scale (RUDAS) score
77 of less than 24 out of 30, and pre-morbid or other musculoskeletal problems affecting gait

78 performance. Ethics approval for this study was approved by the Human Research Ethics
79 Committee (MU-CIRB 2018/144.1207) and (Ref. number 008/2562).

80

81 **2.2. Sample size calculation**

82 The sample size for this study was calculated using G*Power version 3.1 (G power,
83 Germany)²⁴. Time up and go (TUG) and spatiotemporal parameters were used to calculate
84 sample size. Based on the data from a pilot study, the estimated sample to obtain a power of
85 90% with a five percent significance level was 17 participants.

86

87 **2.3. Procedures**

88 The researchers explained the protocol to participants and demonstrated walking on
89 the Force Distribution Measurement/Win FDM device before taking consent. The participants
90 were asked to walk barefoot (control condition) and whilst wearing an EBO and AFO (with
91 shoes), the order of which were randomised. The barefoot condition aimed to investigate the
92 spatiotemporal parameters without any support, and the AFO condition was used as a
93 reference standard management to compare with the EBO. They were required to walk 10
94 meters at their most comfortable speed, and were allowed to use an additional walking aid if
95 needed. Three trials under each condition were performed over a 3 meter walkway, and a 3
96 minute rest was allowed between trials and a 10 minute rest was allowed between conditions.

97

98 **2.4 EBO and AFO interventions**

99 The EBO consisted of an open toe non-slip sock with two straps (Figure 1a, b). The
100 two different lengths of straps are attached on both sides of the sock. A long strap is placed
101 on the medial side and goes across the top of the dorsum of the foot to the opposite side
102 above the lateral malleolus and wraps around the lower leg above the gastrocnemius back to

103 the medial side. The short strap on the lateral side goes across the top of the dorsum of the
104 foot and wraps across the gastrocnemius back to the lateral side. Both straps are fixed with
105 Velcro in front of the tibial tuberosity. The AFO was a non-hinged custom-made Polypropylene
106 Posterior Leaf Spring (Polypropylene PLS), and was chosen and fitted by a qualified
107 practitioner (physician, PT and Prosthetist) which considered the individual participants clinical
108 needs (Figure 1c). The protocol and material used in the AFO production was similar for all
109 participants.

110

111 **2.5. Outcome measures**

112 The TUG is a standard test for testing mobility and balance impairment. This test
113 required participants to stand up, walk 3 meters, make a turn, walk back to the chair, and sit
114 down. The time was recorded from when their buttocks lifted from the chair to when their
115 buttocks touched the seat. During the turn the participants were required to turn toward the
116 unaffected side.

117 Spatiotemporal gait parameters included; velocity, cadence, stride length, step length,
118 stride time, step time, stance time, single support time, and double support time, which were
119 recorded on the Zebris FDM Rehawalk[®] system. The walkway consists of an electronic mat
120 embedded underneath a walkway consisting of 10,240 miniature force sensors, each
121 approximately 0.85 × 0.85 cm, which recorded the foot placements and timings. The stride
122 length and step length were normalized by participants' height.

123 The modified Ashworth scale (MAS) is the most widely used clinical scale used to
124 measure muscle spasticity in the subacute and chronic phases post stroke. The spasticity
125 according to the MAS (0 = no spasticity, 5 = rigidity), was assessed in the hip adductors, knee
126 flexors and extensors, ankle plantar flexors and supinators. In addition, the Fugl-Meyer Motor
127 Assessment-Lower Extremity (FMA-LE) was used to evaluate the motor function. FMA-LE
128 consists of 17 items, with a maximum possible score of 34 points. Each item was answered

129 using a 3-point ordinal scale (0 = cannot perform, 1 = can partially perform, 2 = can fully
130 perform). In addition, the Rowland Universal Dementia Assessment Scale (RUDAS)-Thai
131 version was used to screen cognitive performance. The RUDAS score lower or equal to 23
132 represents a cognitive function impairment. All assessments were completed by trained
133 registered physical therapists.

134 The Quebec user evaluation of satisfaction with assistive technology version 2.0
135 (QUEST 2.0) is a 12-item outcome measure that assesses user satisfaction with the device
136 (8 items), services (4 items), and open-ended questions. The 8 device items and open-ended
137 questions were collated to assess user satisfaction of the EBO.

138

139 **2.6. Data analysis**

140 The general characteristics of participants were analyzed using descriptive statistics.
141 Kolmogorov Smirnov tests were used to identify the distribution of the data and all data were
142 found to be not normally distributed. Friedman tests were performed to determine differences
143 between the conditions for the affected and unaffected sides separately. Where significant
144 differences were seen post hoc Wilcoxon-signed rank test were performed to determine
145 differences between individual conditions for the gait and balance outcome measures. All data
146 were analyzed using SPSS (IBM, USA), and the alpha level was set at 0.05.

147

148 **3. Results**

149 Seventeen individuals (11 males and 6 females) with hemiplegia were recruited. The
150 mean age was 50.82 ± 13.54 years with a mean body mass index of 22.86 ± 2.70 kg/m². The
151 participants characteristics are presented in Table 1.

152

153 **3.1. Gait and balance measures**

154 Friedman tests revealed significant differences between the three conditions for; stride
155 length ($p=0.016$), stride time ($p=0.006$), cadence ($p=0.005$), velocity ($p=0.001$), percentage
156 stance phase on the affected side ($p=0.025$), percentage swing phase on the affected side
157 ($p=0.025$), step length on the unaffected side ($p=0.029$) and percentage pre-swing phase on
158 the unaffected side ($p=0.025$). In addition, the TUG test also showed significant differences
159 between the three conditions ($p=0.001$).

160 Post hoc Wilcoxon Signed Rank test showed differences between the EBO and the
161 control condition with the EBO showing an increase in stride length ($p=0.009$), percentage
162 swing phase on the affected side ($p=0.003$), and step length on the unaffected side ($p=0.035$).
163 Moreover, the EBO showed a decrease in the percentage of stance phase on the affected
164 side ($p=0.01$), percentage of pre-swing phase on the unaffected side ($p=0.035$), and TUG test
165 ($p=0.008$). Significant differences were also seen between the EBO and AFO conditions with
166 the EBO showing a greater stride length ($p=0.008$), cadence ($p=0.004$), velocity ($p=0.001$),
167 and step length on the unaffected side ($p=0.031$), with a shorter stride time ($p=0.009$) and
168 TUG test time ($p=0.001$). In addition, the AFO increased velocity ($p=0.044$) when compare to
169 the control condition. The AFO showed higher TUG test time when compare to control
170 condition, but it was not significant difference (Table 3, Figure 2-3).

171

172 **3.2. User Evaluation of Satisfaction**

173 The QUEST 2.0 and open-ended questions showed that participants were most
174 satisfied with the weight of the EBO (Median=5, IQR=0) and were least satisfied with the
175 durability (Median=3, IQR=1) (Table 2). The open ended questions of QUEST showed positive
176 comments from participants about the EBO associated with the weight and ability to walk
177 freely, better than the AFO (100%). The participants reported that they wanted to use the EBO
178 at home in their daily activities (82.4%). However, 17.6% reported they did not want to use the
179 device with the most common reasons being they needed more time to practice with the EBO,

180 with some participants not wanting to use any assistive device. Additional comments included
181 that the EBO felt like wearing a pair of socks, which was comfortable and supported firmly at
182 the ankle, and made the participants feel more confident during walking (100%). They also
183 perceived that the EBO aided their walking pattern and corrected their posture and helped
184 their speed (100%). Moreover, they reported that their ankle and toe twitch during walking
185 were decreased (58.8%).

186

187 **4. Discussion**

188 Assistive technology for stroke survivors has been developed for decades. Several
189 studies have demonstrated that ankle supports can alter gait and balance performance in this
190 population ^{7,10-15,17,20,22,23}. Several types of ankle support are available which include ankle foot
191 orthosis (AFO), which are prescribed to stroke survivors to support their ambulation. However,
192 the AFO still has some limitations, especially limiting ankle movement during walking ^{12,17,19,21}.
193 The purpose of this study was to investigate the effect of an elastic band orthosis on gait and
194 balance performance in stroke survivors and to provide a comparison with AFOs.

195

196 **4.1 Gait and balance performance**

197 Gait and balance performance was assessed through spatiotemporal gait parameters
198 and the TUG test. Significant differences were found in velocity, cadence, stride length, stride
199 time, stance phase and swing phase on the affected side, and pre-swing and step length on
200 the unaffected side, and the TUG test when using the EBO. These findings are in line with
201 previous studies whereby step length on the unaffected side was improved after applying both
202 rigid and elastic ankle supports ^{14,22,25}. However, the EBO significantly improved
203 spatiotemporal gait parameters when compared with the AFO. This implies that the EBO
204 encourages weight bearing and gait performance during stance phase on the affected side,
205 and longer step lengths on the unaffected side. When comparing the two devices the AFO

206 limits the amount of ankle dorsiflexion which affected reaching and gait performance ^{15,17,26}.
207 Particularly during stance, limited ankle dorsiflexion in the affected side could lead to a shorter
208 step length ²⁷, and stride length in the AFO when compared to the control condition and EBO.
209 Whereas the EBO offers little restriction of dorsiflexion as this is made from elasticated fabric.

210 The EBO subtly altered the proportions of stance phase and swing phase of the
211 affected side moving these closer to the normal stance and swing proportions (60:40) when
212 compared to the control and AFO conditions. The decrease of pre-swing phase on the
213 unaffected side while walking using the EBO indicated that the transition phase between
214 stance and swing on the unaffected side was improved. This phenomenon might be related to
215 improved stability of the affected side during the stance phase, and lead the unaffected side
216 to become more efficient during propulsion ^{10,13,14,23}. These affects are associated with force
217 from the elastic bands within the EBO which provide some supportive properties for the ankle
218 joint during single limb loading in stance phase on the affected side, and might lead to a longer
219 step length of the unaffected side. Collectively this led to the improvement in stride time,
220 cadence, velocity and TUG test time in this sample of stroke survivors. However, the elastic
221 properties and the optimum force needed for the best function needs to be further explored.

222

223 **4.2. User Evaluation of Satisfaction**

224 The QUEST 2.0 questionnaire was used to evaluate satisfaction with the EBO. The
225 questionnaire was selected as it has previously been presented to be a valid measure of
226 satisfaction with assistive devices ²⁸. Overall, patients were quite satisfied with the EBO
227 (Median=4, IQR=1). All participants supported that the EBO could be used to improve balance
228 during walking. It encouraged participants to walk confidently, and their comments seemed to
229 relate to the findings from the gait and balance performance measures. Compared to the
230 control condition, the EBO was reported to support the affected ankle in dorsiflexion with
231 eversion, which promoted patients' ability to clear their toe from the floor and the participants

232 reported that the EBO felt lighter than the AFO. It is noteworthy that polypropylene
233 development and hybrid AFOs made of polypropylene and fabric have been explore to
234 facilitate the gait in stroke survivors²⁸⁻³⁰. The lighter weight orthoses showed a higher level of
235 satisfaction which supports the current findings from the EBO. While the majority of items
236 showed users were quite satisfied with the EBO (7 out of 8 items), the durability of the EBO
237 presented as more or less satisfied (1 out of 8 items). Following the concept of the HAAT
238 (Human, Activity, Assistive Technology) model evaluated by QUEST 2.0, the EBO improved
239 the gait and balance performance for stroke survivors during walking^{8,9}. Participants (82.4%)
240 agreed that the EBO was suitable for their home environment and wanted to use the EBO in
241 their daily living. The EBO seems to offer better results than the AFO when considering both
242 the gait and balance performance and comments from this sample of stroke survivors. A
243 comparison of the satisfaction when wearing AFOs and EBOs using the QUEST 2.0 might be
244 considered in further investigations.

245 It has been presented that the Fugl-Meyer score of lower extremity function cut-off
246 score for high level of mobility function in chronic stroke survivors is 21 out of 35³¹. Using this
247 score all participants in this current study were deemed to have a high level of mobility function
248 (Table 1). Further investigation in individuals with different levels of function to further
249 understand the generalizability of these results is recommended.

250

251 **5. Conclusion**

252 The EBO seems to improve TUG, gait velocity, cadence, stride length, stride time,
253 stance phase and swing phase on the affected side, and pre-swing and step length on the
254 unaffected side over both the AFO and control conditions, which are reflected by the user
255 evaluations of satisfaction. Therefore, the EBO could be used in clinical and community
256 settings, and could mitigate against some of the limitations reported in the use of AFOs in
257 stroke survivors.

258

259 **Figure 1** The Elastic Band Orthosis (EBO) (The A band contributes the inversion and the B
260 band contributes the eversion) (a-b) and Polypropylene Posterior Leaf Spring (Polypropylene
261 PLS) (c)

262

263 **Figure 2** Presented the median (IQR) among three groups (Control, AFO and EBO). The post
264 hoc Wilcoxon Signed rank test identified the significant difference between pairs.

265

266 **Figure 3** Presented the median (IQR) of stride time (sec) and velocity (km/hr.) among three
267 groups (Control, AFO and EBO). The post hoc Wilcoxon Signed rank test identified the
268 significant difference between pairs. (* $P < 0.05$, ** $P < 0.005$)

269

270 **Table 1** Present the specific conditions and lower limb Modified Ashworth Scale (MAS)

271

272 **Table 2** Present the Quebec User Evaluation of Satisfaction with assistive Technology version
273 2.0 (QUEST-2.0), Assistive device section, from participants after used EBO

274

275 **Table 3** Present the spatiotemporal parameters and TUG among 3 conditions (Control, AFO
276 and EBO)

277

278

279

280

281

282

283

284

285

287 **References**

- 288 1. Hanchaiphibookkul S, Pongvarin N, Nidhinandana S, et al. Prevalence of stroke and stroke risk
289 factors in Thailand: Thai Epidemiologic Stroke (TES) Study. *J Med Assoc Thai*. 2011;94(4):427-
290 436.
- 291 2. Suwanwela NC. Stroke epidemiology in Thailand. *J Stroke*. 2014;16(1):1-7.
- 292 3. Platts MM, Rafferty D, Paul L. Metabolic cost of over ground gait in younger stroke patients
293 and healthy controls. *Med Sci Sports Exerc*. 2006;38(6):1041-1046.
- 294 4. Dajpratham P, Kuptniratsaikul V, Kovindha A, Kuptniratsaikul PS, Dejnuntarat K. Prevalence
295 and management of poststroke spasticity in Thai stroke patients: a multicenter study. *J Med*
296 *Assoc Thai*. 2009;92(10):1354-1360.
- 297 5. Wei TS, Liu PT, Chang LW, Liu SY. Gait asymmetry, ankle spasticity, and depression as
298 independent predictors of falls in ambulatory stroke patients. *PLoS One*.
299 2017;12(5):e0177136.
- 300 6. Li S. Ankle and Foot Spasticity Patterns in Chronic Stroke Survivors with Abnormal Gait. *Toxins*
301 *(Basel)*. 2020;12(10).
- 302 7. Sankaranarayan H, Gupta A, Khanna M, Taly AB, Thennarasu K. Role of ankle foot orthosis in
303 improving locomotion and functional recovery in patients with stroke: A prospective
304 rehabilitation study. *J Neurosci Rural Pract*. 2016;7(4):544-549.
- 305 8. Lim YM, Kim SK, Yoo DH, Kim H. Effects of assistive technology-based occupational therapy on
306 community-dwelling people recovering from stroke. *Assist Technol*. 2020:1-8.
- 307 9. Giesbrecht E. Application of the Human Activity Assistive Technology model for occupational
308 therapy research. *Aust Occup Ther J*. 2013;60(4):230-240.
- 309 10. Daryabor A, Arazpour M, Aminian G. Effect of different designs of ankle-foot orthoses on gait
310 in patients with stroke: A systematic review. *Gait Posture*. 2018;62:268-279.

- 311 11. Nikamp CDM, Hobbelink MSH, van der Palen J, Hermens HJ, Rietman JS, Buurke JH. A
312 randomized controlled trial on providing ankle-foot orthoses in patients with (sub-)acute
313 stroke: Short-term kinematic and spatiotemporal effects and effects of timing. *Gait Posture*.
314 2017;55:15-22.
- 315 12. Totah D, Menon M, Jones-Hershinow C, Barton K, Gates DH. The impact of ankle-foot orthosis
316 stiffness on gait: A systematic literature review. *Gait Posture*. 2019;69:101-111.
- 317 13. Dahera N. LS, Yang YJ. Effects of elastic band orthosis (aider) on balance and gait in chronic
318 stroke patients. *Phys Ther Rehabil Sci*. 2013;2:81-86.
- 319 14. Gok H, Kucukdeveci A, Altinkaynak H, Yavuzer G, Ergin S. Effects of ankle-foot orthoses on
320 hemiparetic gait. *Clin Rehabil*. 2003;17(2):137-139.
- 321 15. Cakar E, Durmus O, Tekin L, Dincer U, Kiralp MZ. The ankle-foot orthosis improves balance and
322 reduces fall risk of chronic spastic hemiparetic patients. *Eur J Phys Rehabil Med*.
323 2010;46(3):363-368.
- 324 16. Waterval NFJ, Brehm MA, Harlaar J, Nollet F. Energy cost optimized dorsal leaf ankle-foot-
325 orthoses reduce impact forces on the contralateral leg in people with unilateral plantar flexor
326 weakness. *Gait Posture*. 2022;92:71-76.
- 327 17. Geboers JF, Wetzelaer WL, Seelen HA, Spaans F, Drost MR. Ankle-foot orthosis has limited
328 effect on walking test parameters among patients with peripheral ankle dorsiflexor paresis. *J*
329 *Rehabil Med*. 2002;34(2):80-85.
- 330 18. Nikamp C, Buurke J, Schaake L, van der Palen J, Rietman J, Hermens H. Effect of long-term use
331 of ankle-foot orthoses on tibialis anterior muscle electromyography in patients with sub-acute
332 stroke: A randomized controlled trial. *J Rehabil Med*. 2019;51(1):11-17.
- 333 19. Geboers JF, Drost MR, Spaans F, Kuipers H, Seelen HA. Immediate and long-term effects of
334 ankle-foot orthosis on muscle activity during walking: a randomized study of patients with
335 unilateral foot drop. *Arch Phys Med Rehabil*. 2002;83(2):240-245.

- 336 20. Mizuno S, Sonoda S, Takeda K, Maeshima S. Effect of muscle tone on ankle kinetics during gait
337 with ankle-foot orthoses in persons with stroke. *Top Stroke Rehabil.* 2017;24(8):567-572.
- 338 21. Tyson SF, Thornton HA. The effect of a hinged ankle foot orthosis on hemiplegic gait: objective
339 measures and users' opinions. *Clin Rehabil.* 2001;15(1):53-58.
- 340 22. Hwang YI, Yoo WG, An DH. Effects of the Elastic Walking Band on gait in stroke patients.
341 *NeuroRehabilitation.* 2013;32(2):317-322.
- 342 23. Patil P, Rao S. Effects of Thera-Band(R) elastic resistance-assisted gait training in stroke
343 patients: a pilot study. *Eur J Phys Rehabil Med.* 2011;47(3):427-433.
- 344 24. Faul F, Erdfelder E, Lang AG, Buchner A. G*Power 3: a flexible statistical power analysis
345 program for the social, behavioral, and biomedical sciences. *Behav Res Methods.*
346 2007;39(2):175-191.
- 347 25. Rao N, Wening J, Hasso D, et al. The effects of two different ankle-foot orthoses on gait of
348 patients with acute hemiparetic cerebrovascular accident. *Rehabil Res Pract.*
349 2014;2014:301469.
- 350 26. Hsu CC, Huang YK, Kang JH, et al. Novel design for a dynamic ankle foot orthosis with motion
351 feedback used for training in patients with hemiplegic gait: a pilot study. *J Neuroeng Rehabil.*
352 2020;17(1):112.
- 353 27. Kesikburun S, Yavuz F, Guzelkucuk U, Yasar E, Balaban B. Effect of ankle foot orthosis on gait
354 parameters and functional ambulation in patients with stroke. *Turk J Phys Med Rehabil.*
355 2017;63(2):143-148.
- 356 28. Magnusson L, Ramstrand N, Fransson EI, Ahlstrom G. Mobility and satisfaction with lower-
357 limb prostheses and orthoses among users in Sierra Leone: a cross-sectional study. *J Rehabil*
358 *Med.* 2014;46(5):438-446.
- 359 29. Do KH, Song JC, Kim JH, et al. Effect of a hybrid ankle foot orthosis made of polypropylene and
360 fabric in chronic hemiparetic stroke patients. *Am J Phys Med Rehabil.* 2014;93(2):130-137.

361 30. Bregman DJ, De Groot V, Van Diggele P, Meulman H, Houdijk H, Harlaar J. Polypropylene ankle
362 foot orthoses to overcome drop-foot gait in central neurological patients: a mechanical and
363 functional evaluation. *Prosthet Orthot Int.* 2010;34(3):293-304.

364 31. Kwong PWH, Ng SSM. Cutoff Score of the Lower-Extremity Motor Subscale of Fugl-Meyer
365 Assessment in Chronic Stroke Survivors: A Cross-Sectional Study. *Arch Phys Med Rehabil.*
366 2019;100(9):1782-1787.

367

368

369



374

375 (a)

376

377

378

379

380

381

382

383

384

385

386

387



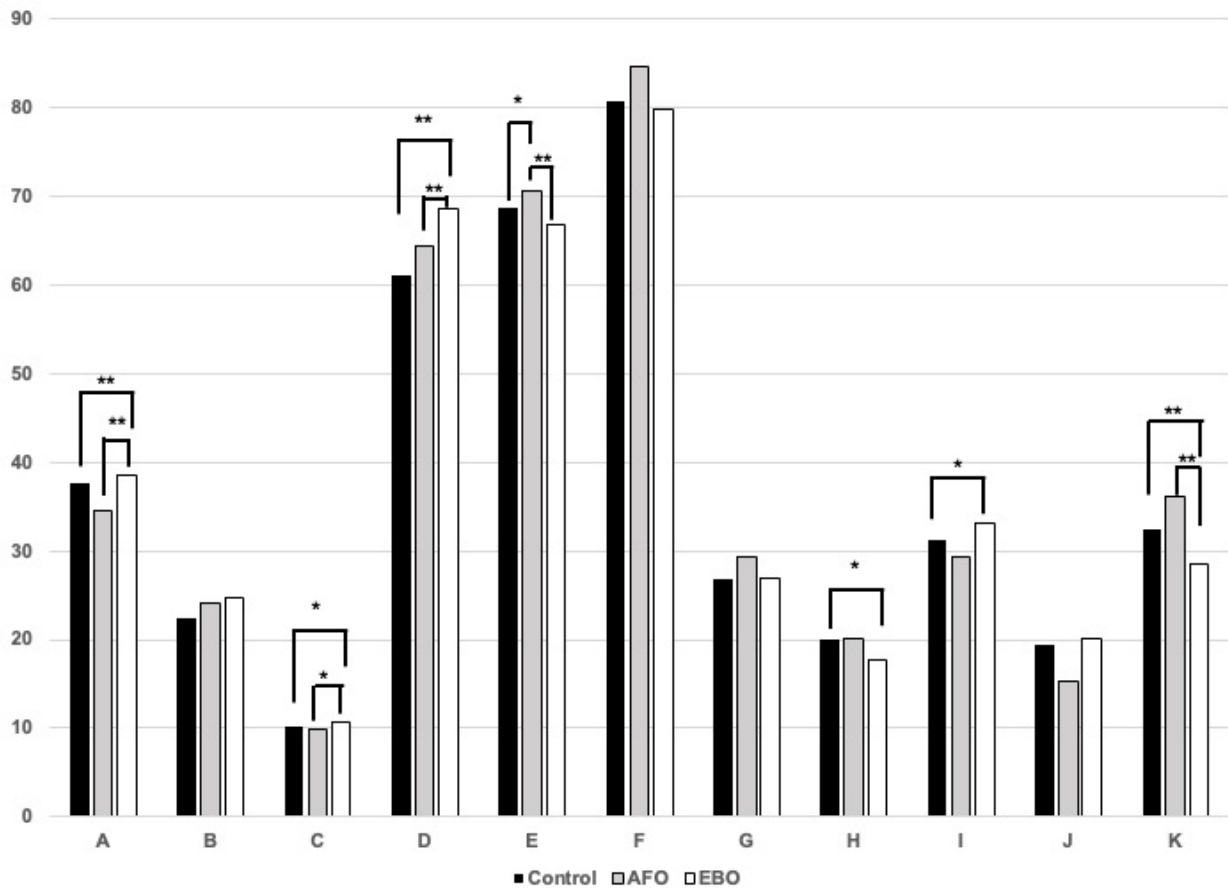
(b)

(c)



388 **Figure 1** The Elastic Band Orthosis (EBO) (The A band contributes the inversion and the B
389 band contributes the eversion) (a-b) and Polypropylene Posterior Leaf Spring (Polypropylene
390 PLS) (c)

391



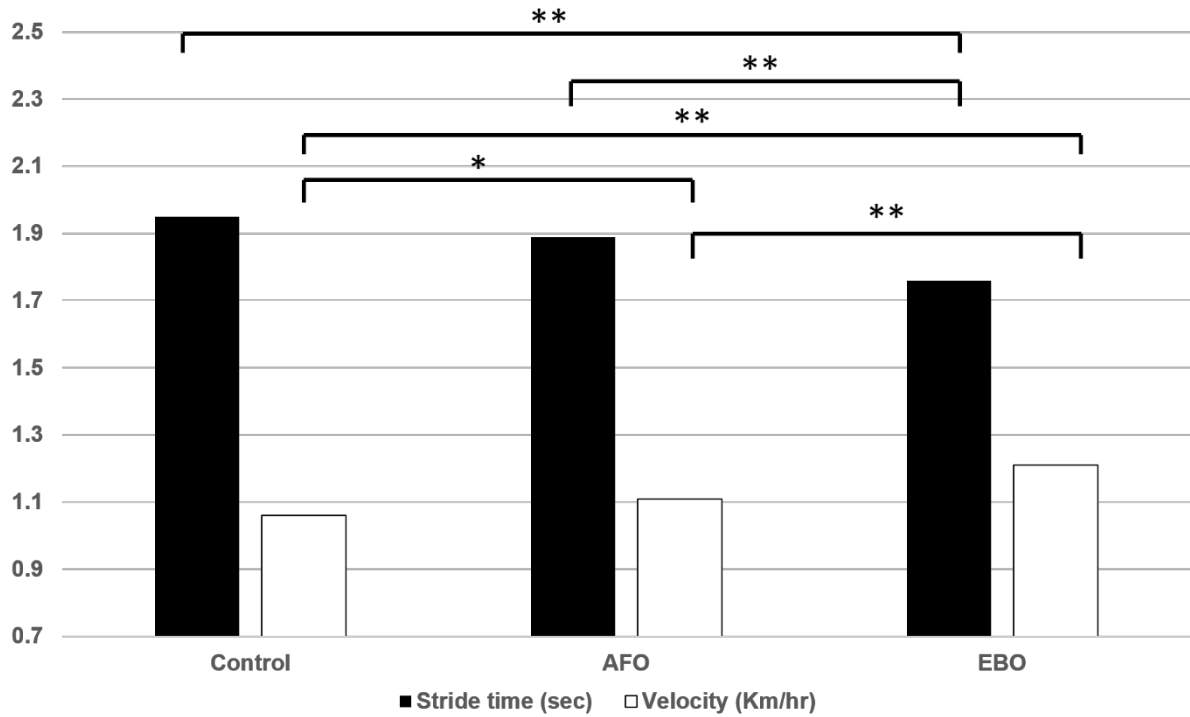
392

393 **Figure 2** Presented the median (IQR) among three groups (Control, AFO and EBO). The post
 394 hoc Wilcoxon Signed rank test identified the significant difference between pairs.

395 (* P<0.05, ** P<0.005, A= Stride length (%), B= Step length affected side (%), C= Step length unaffected
 396 side (%), D= Cadence (step), E= Stance phase affected side (% gait cycle), F= Stance phase unaffected
 397 side (% gait cycle), G= Pre-swing phase affected side (%), H= Pre-swing phase unaffected side (%), I=
 398 Swing phase affected side (%), J= Swing phase unaffected side (%), and K= Time up and go (TUG)
 399 (seconds))

400

401



402

403 **Figure 3** Presented the median (IQR) of stride time (sec) and velocity (km/hr.) among three
 404 groups (Control, AFO and EBO). The post hoc Wilcoxon Signed rank test identified the
 405 significant difference between pairs. (* P<0.05, ** P<0.005)

406

407

408 **Table 1** Present the specific conditions and lower limb Modified Ashworth Scale (MAS)

Conditions	Mean ± SD	Number	Percent (%)
Diagnosis			
Ischemic stroke		15	88.20
Hemorrhagic stroke		2	11.80
Duration of onset (months)	10.65±16.63		
Affected side			
Left		9	52.90
Right		8	47.10
Modified Ashworth Scale (MAS):			
Ankle planta flexor and supinator		7	41.20
Spasticity Level 1		10	58.80
Spasticity Level 2			
Fugl-Meyer Motor Assessment (FMA)	25.00 ± 3.20		
Lower Extremity) (total = 34)	(Min = 18 - Max = 29)		
Rowland Universal Dementia	29.26 ± 1.28		
Assessment Scale (RUDAS, total 30)	(Min = 25 – Max = 30)		

409

410

411 **Table 2** Present the Quebec User Evaluation of Satisfaction with assistive Technology version
 412 2.0 (QUEST-2.0), Assistive device section, from participants after used EBO

QUEST (Version-2.0) Assistive device	Score EBO from participants	
	Median	IQR
1. the dimensions (size, height, length, width) of your assistive device?	5	0.5
2. the weight of your assistive device?	5	0
3. the ease in adjusting (fixing, fastening) the parts of your assistive device?	4	1.5
4. how safe and secure your assistive device is?	4	1
5. the durability (endurance, resistance to wear) of your assistive device?	3	1
6. how easy it is to use your assistive device?	4	1
7. how comfortable your assistive device is?	4	1
8. how effective your assistive device is (the degree to which your device meets your needs)?	4	1
Overall score	4	1

413

414

415 **Table 3** Present the spatiotemporal parameters and TUG among 3 conditions (Control, AFO
 416 and EBO)

Spatiotemporal gait parameters	Median (IQR)			p-value ^a
	Control	AFO	EBO	
Velocity (km/h)	1.06 (0.99)	1.11 (0.82)	1.21 (0.98)	0.001**
Stride length (%)	37.73 (17.70)	34.64 (15.14)	38.50 (17.75)	0.016*
Step length (%) -Affected side -Unaffected side	22.33 (6.84) 10.27 (11.08)	24.12 (6.97) 9.92 (15.90)	24.64 (11.38) 10.69 (15.27)	0.51 0.029*
Cadence (step/minute)	61.17 (33.20)	64.37 (24.13)	68.62 (27.00)	0.005*
Stride time (sec)	1.95 (1.05)	1.89 (0.78)	1.76 (0.79)	0.006*
Stance phase (% gait cycle) -Affected side -Unaffected side	68.70 (11.75) 80.68 (12.56)	70.66 (12.29) 84.66 (11.62)	66.77 (11.83) 79.88 (11.35)	0.025* 0.33
Pre-swing phase (%) -Affected side -Unaffected side	26.81 (15.54) 20.11 (7.15)	29.34 (13.79) 20.12 (10.51)	26.90 (17.24) 17.8 (7.31)	0.66 0.025*
Swing phase (% gait cycle) -Affected side -Unaffected side	31.30 (11.75) 19.32 (12.56)	29.34 (12.30) 15.34 (11.62)	33.23 (11.82) 20.12 (11.31)	0.025* 0.33
TUG score (seconds)	32.40 (24.23)	36.05 (22.26)	28.60 (23.81)	0.001**

417

418 ^a Friedman test, IQR = Interquartile Range, * P<0.05, ** P<0.005

419

420

421

422

423

424

425

426

427

428

429

430